

Extracellular Matrix Analogues for the Pre-Clinical Handling and Transplantation of Cells

ETP on Nanomedicine Webinar
4th October 2016



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**Brighton Studies in Tissue-mimicry and Aided Regeneration
(*BrightSTAR*)**

**Brighton Centre for Regenerative Medicine
School of Pharmacy & Biomolecular Sciences**



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A New Generation of Biomaterials: From Tissue Re-Placement to Tissue Re-generation

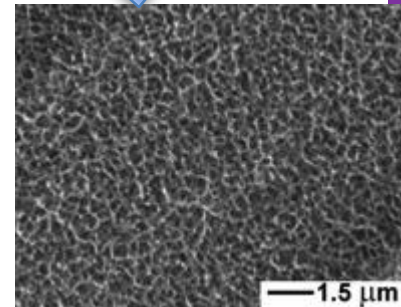
Tissue Replacement



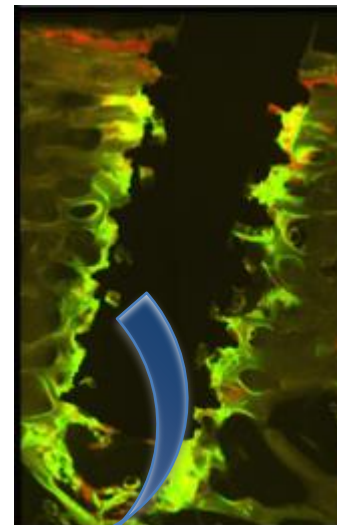
**Adverse
Reactions**



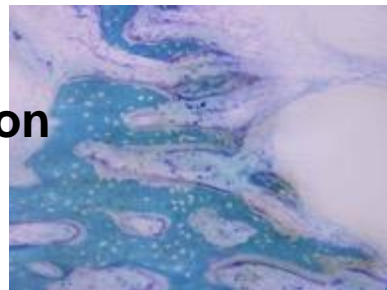
Surface Modification



**Tissue
Integration**



Tissue Regeneration

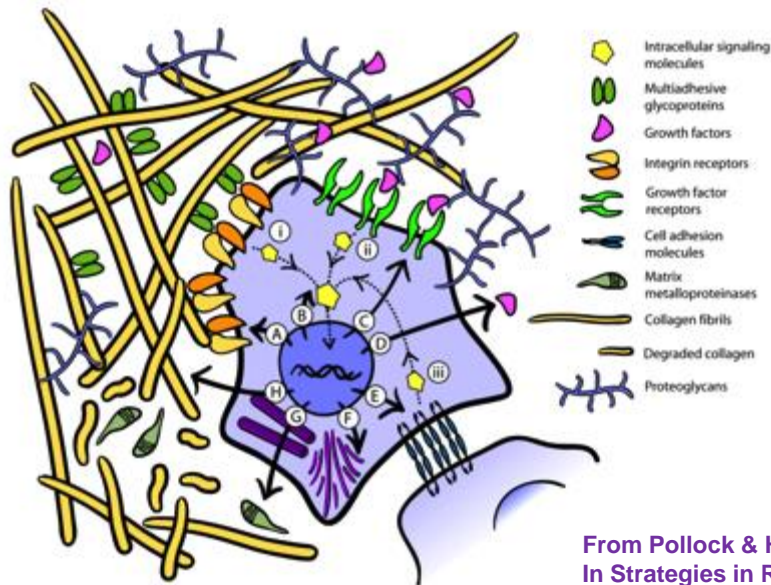


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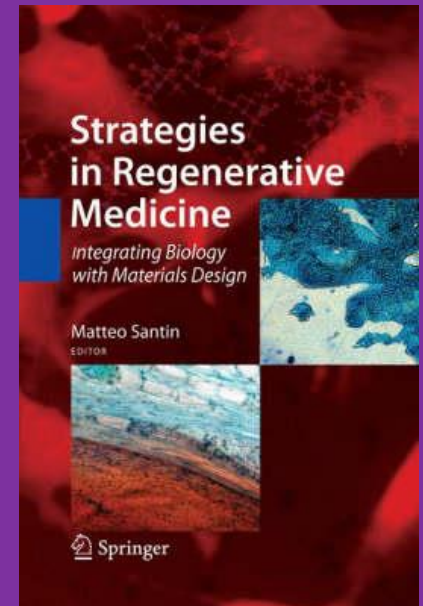
Tissue Microenvironment

- **Modern synthetic biomaterials** fully integrating molecular cues mimicking certain aspects of structure or function of natural extracellular microenvironments

MP Lutolf, JA Hubbell, 2005,
Nat Biotechnol 23 (1): 47-55



From Pollock & Healy
In *Strategies in Regenerative Medicine*
M Santin ed, Springer 2009, Chapter 4



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The Extracellular Matrix Analogue Concept

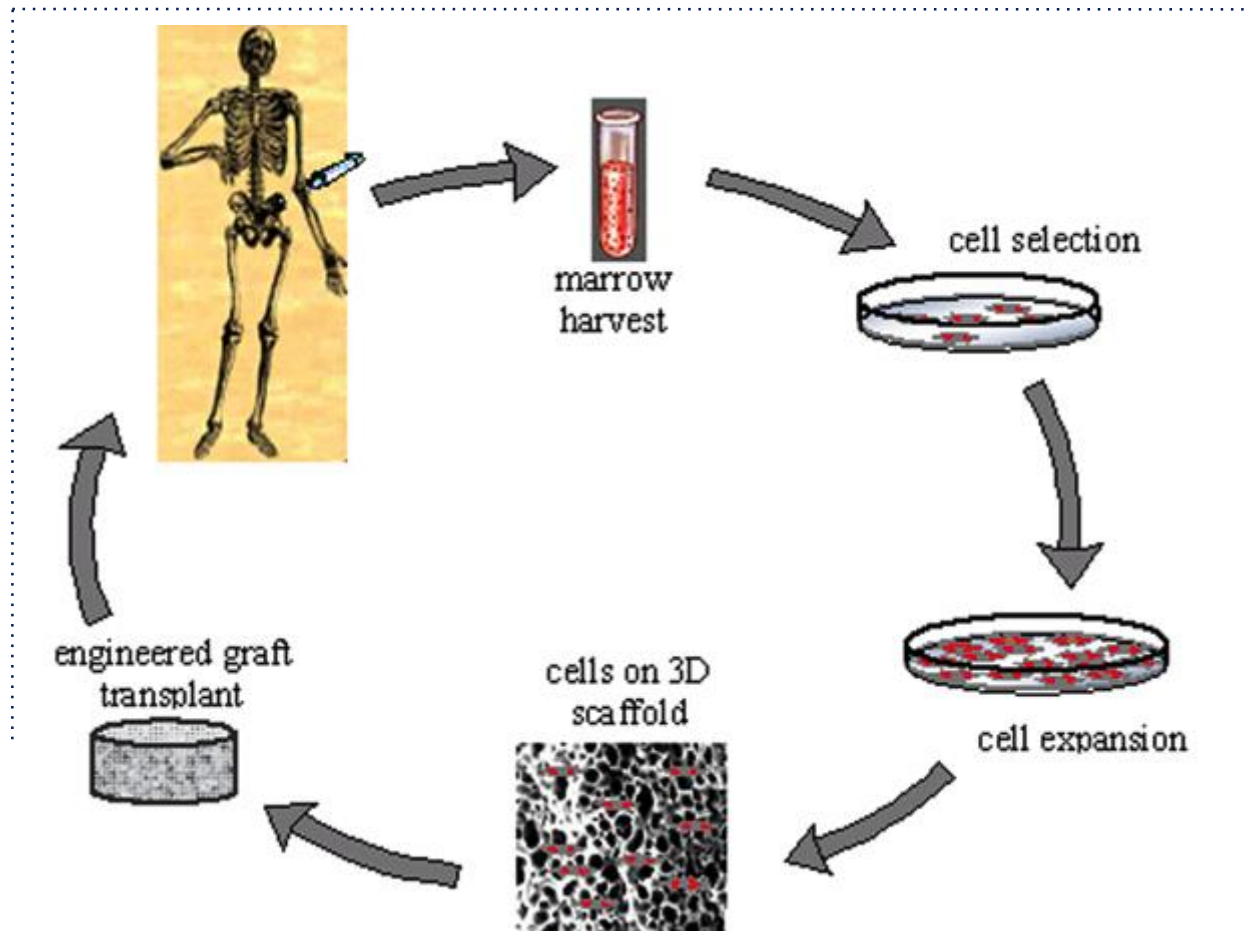
- Extracellular matrix analogues (EMA) are biomaterials that mimic in various ways the environment around bodily cells, with additional features that lead to desired developments, are obtained through a synthetic route are considered to be the new frontiers of biomimetic/bioactive biomaterials. They will be able to **control cell activities and tissue regeneration at nano-/micro-scale level.**

Horizon 2020 Roadmap for Biomaterials

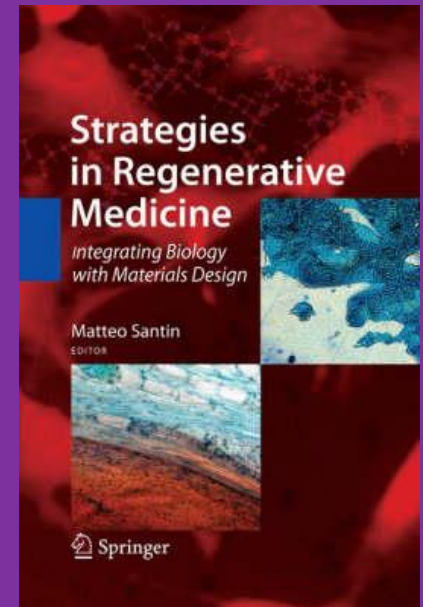
- Types of EMA
 - Nanostructured Biomimetic Materials
 - Bioactive Analogues of Growth Factors (Synthetic Pro-Morphogens)



The Tissue Engineering Paradigm



From Scaglione & Quarto
In *Strategies in Regenerative Medicine*
M Santin ed, Springer 2009, Chapter 15



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Biocompetent Dendrons

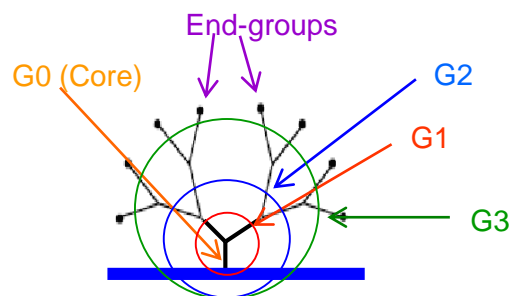
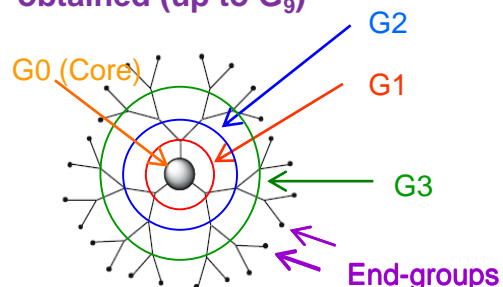
**A Synthetic Biomaterial Platform to Mimic
the Histological Lattice**



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Dendrimeric Systems and Applications

- Dendrimers (Greek: δένδρον, tree) are hyperbranched polymers
- Dendritic structures with different branching generations (G_n) can be obtained (up to G_9)



- Dendrimer types
 - Poly(amido amine) [PAMAM]
 - Poly(ϵ -lysine)
 - Poly(ethylene glycol)
 - Polysaccharides-based
 - Nucleic acid-based
- Biomedical applications
 - Drug/gene carriers (Non viral carrier for *in vitro* cell transfection, Superfect™)
 - Contrast agents
 - Fibroblast spheroids (RGD-PAMAM)

Al Jamal, K. T. et al, 2005,
Advanced Drug Delivery Reviews
57(15), 2238-2270.

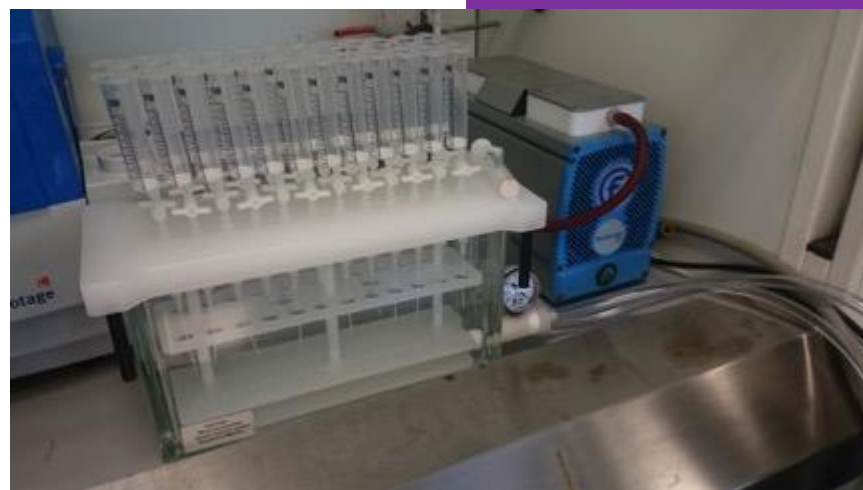
Duncan, R. & Izzo, L. 2005,
Advanced Drug Delivery Reviews,
57(15), 2215-2237

Tang M.X. et al. 1996,
Bioconjugate Chemistry 7, 703-714



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Dendron Synthesis Scale up



Microwave =
~7mins coupling

Manual = 30mins
coupling

1 Syringe: 25%
yield = ~250mg

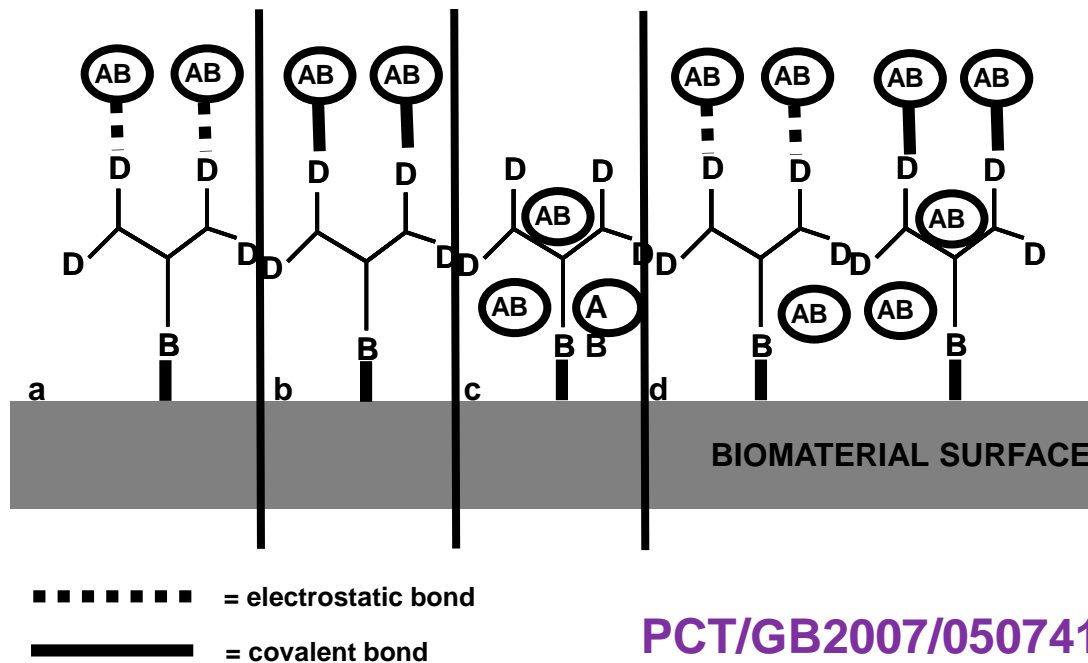
24 X Scale Up

24 Syringe =
~6000mg



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Biomimetic Dendrons as Surface Functionalisation Macromolecules

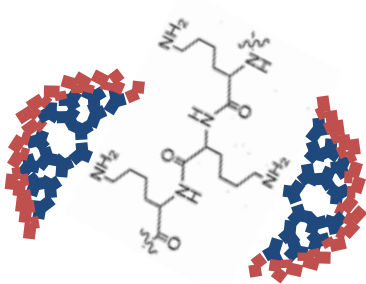


PCT/GB2007/050741

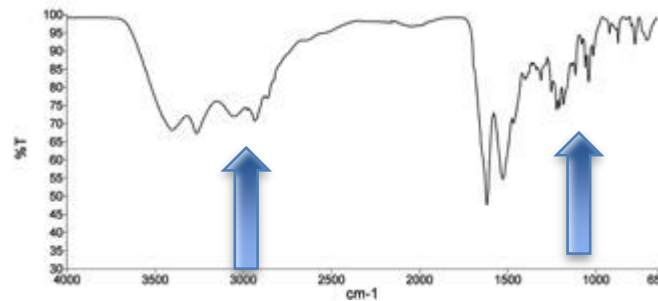


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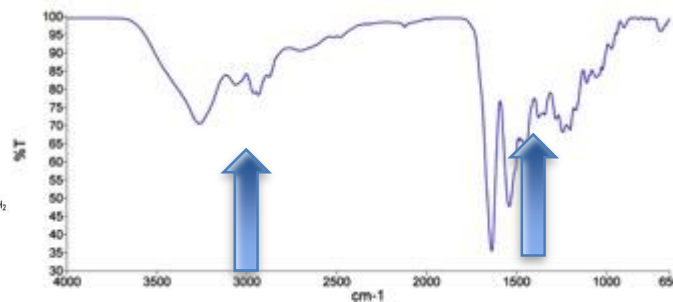
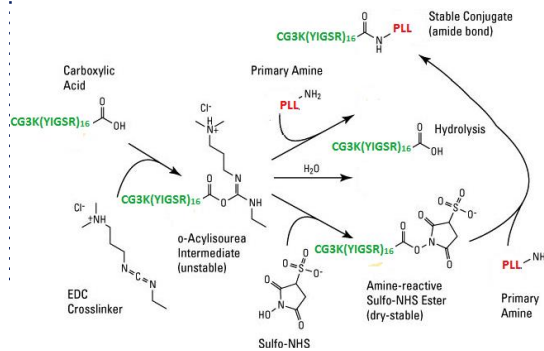
Dendron-modified poly(ϵ -lysine) substrates



1% mol/-NH₂ mol



poly(K)



RG₃K(YIGSR)₁₆-poly(K)



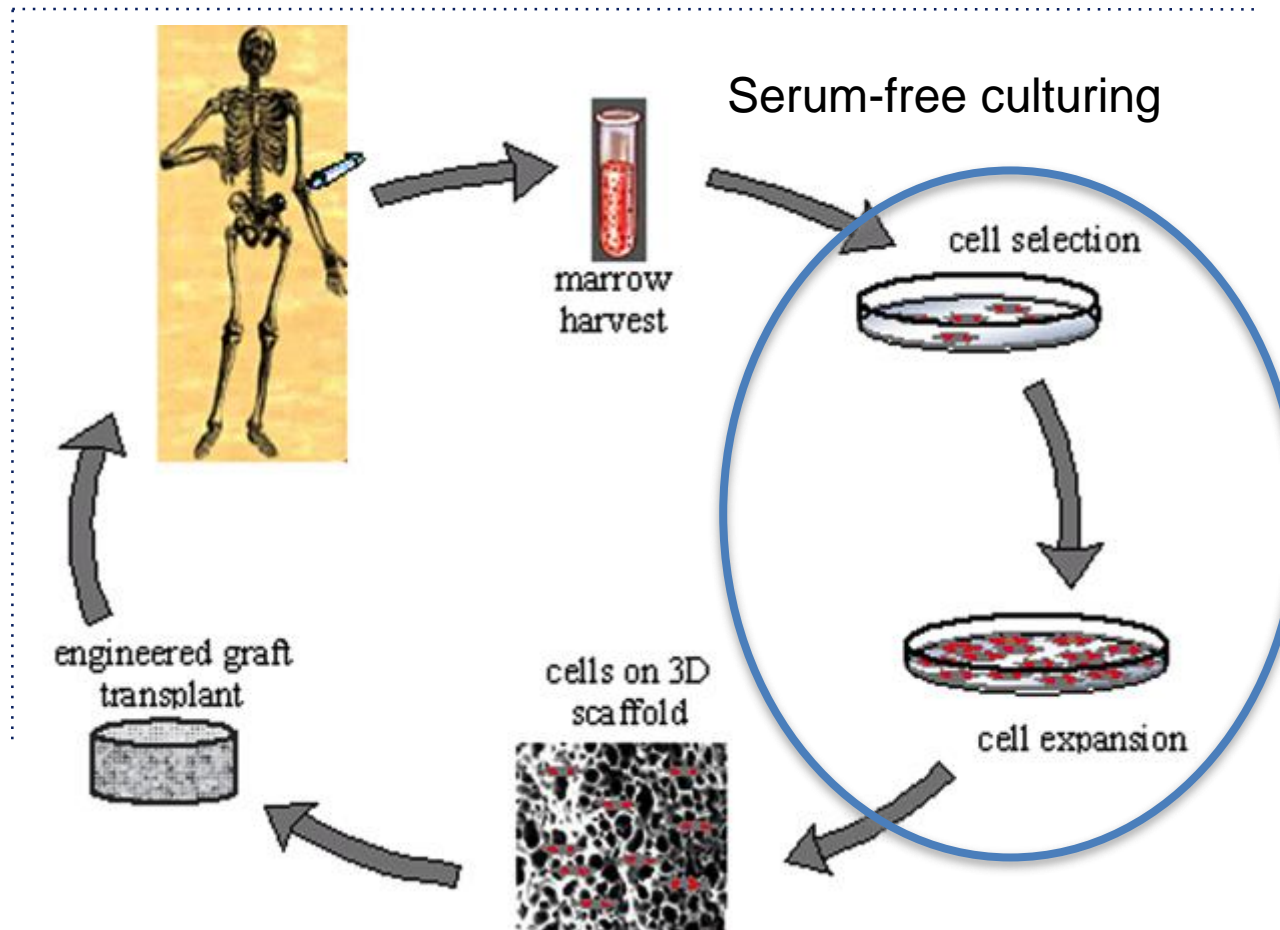
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Extracellular Matrix Analogues for the Pre-clinical Handling of Cells

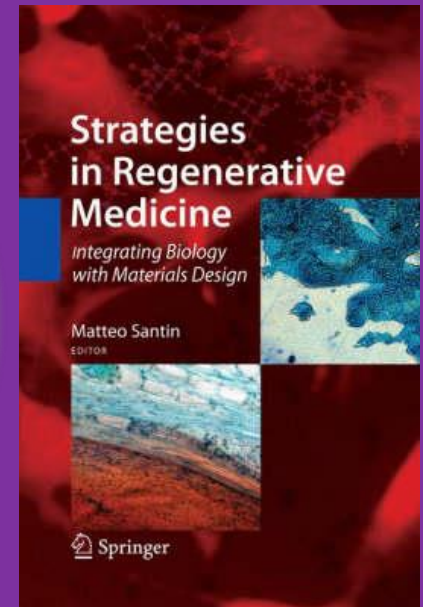


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The Tissue Engineering Paradigm

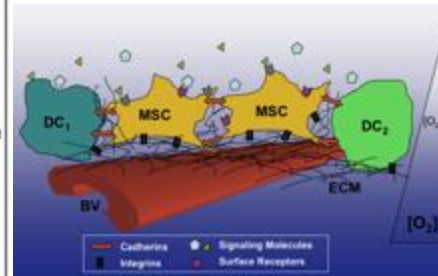
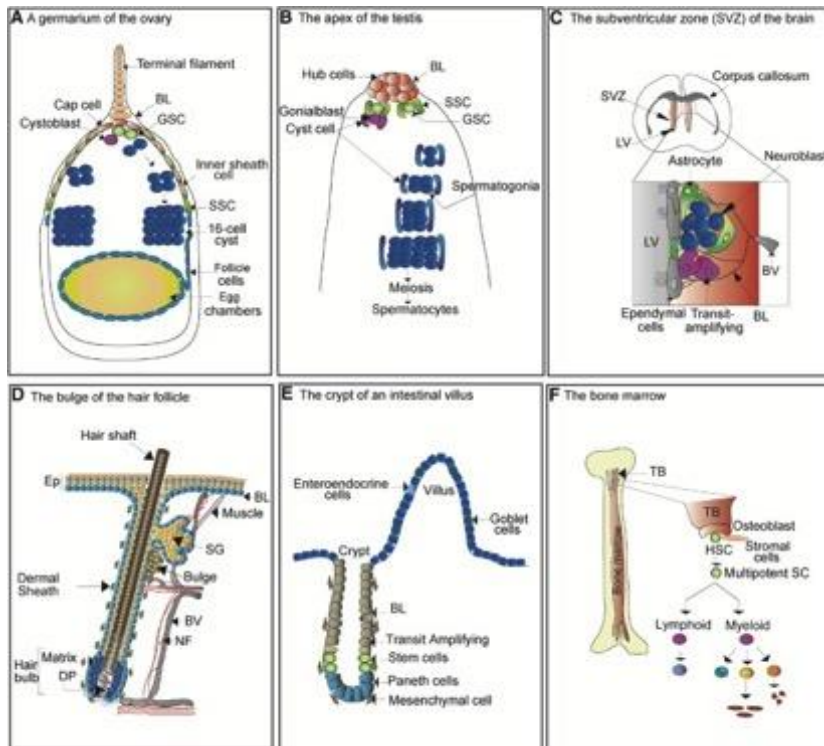


From Scaglione & Quarto
In *Strategies in Regenerative Medicine*
M Santin ed, Springer 2009, Chapter 15

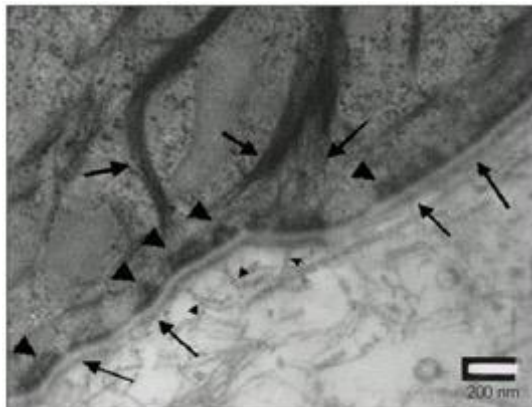
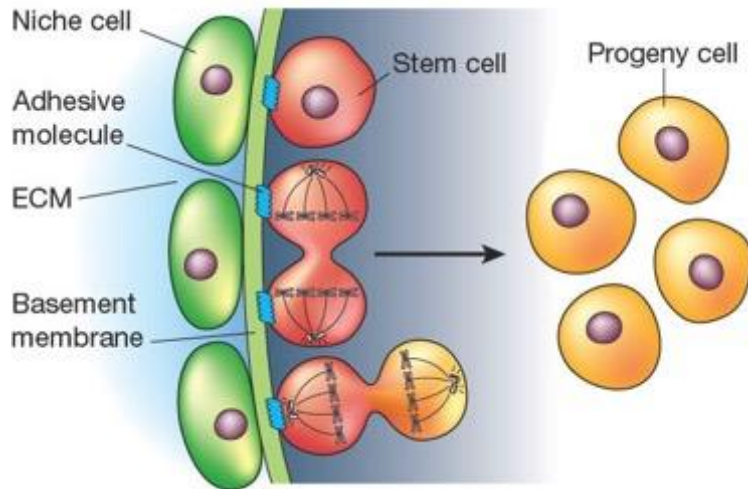


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Types of Adult Stem Cell Niches



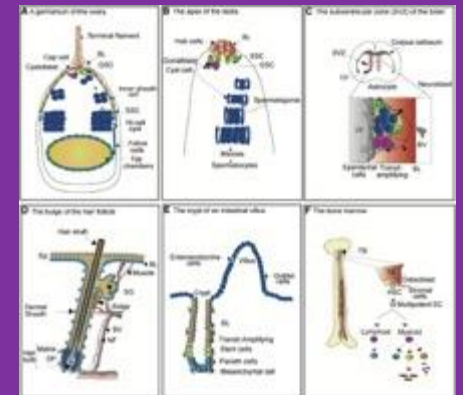
The Basement Membrane



BMS ultrastructure

The major constituents of all BMs are:

- collagen IV
- laminins
- nidogen/entactin
- proteoglycans



Poly(K) derivatisation method:
 Activation of dendritic carboxyl groups by
 10mM N-hydroxysulfossuccinimide (sulfo-NHS)
 4mM 1-ethyl-3-(dimethylaminopropyl) carbodiimide (EDC)
 Poly(K) (70,000-150,000)
 concentration: 0.1% (w/v)
 Dendron concentration: 0.1% (w/v)
 1 hour, room temperature.

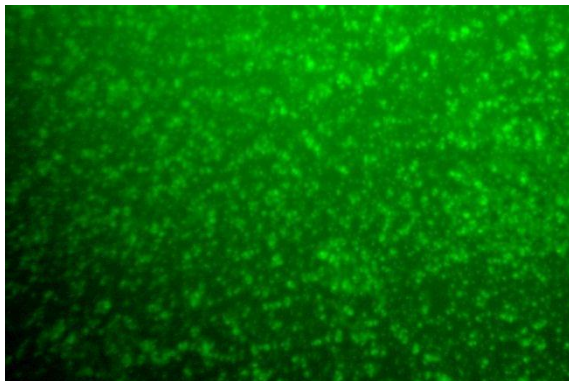


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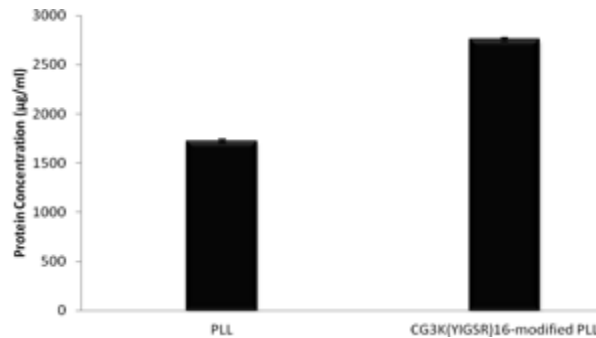
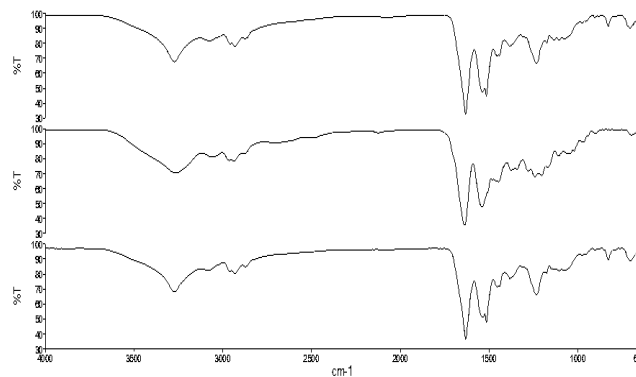
Dendron-modified poly(ϵ -lysine) substrates



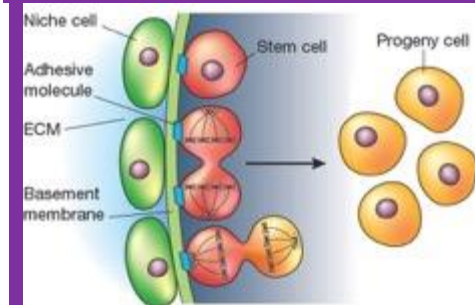
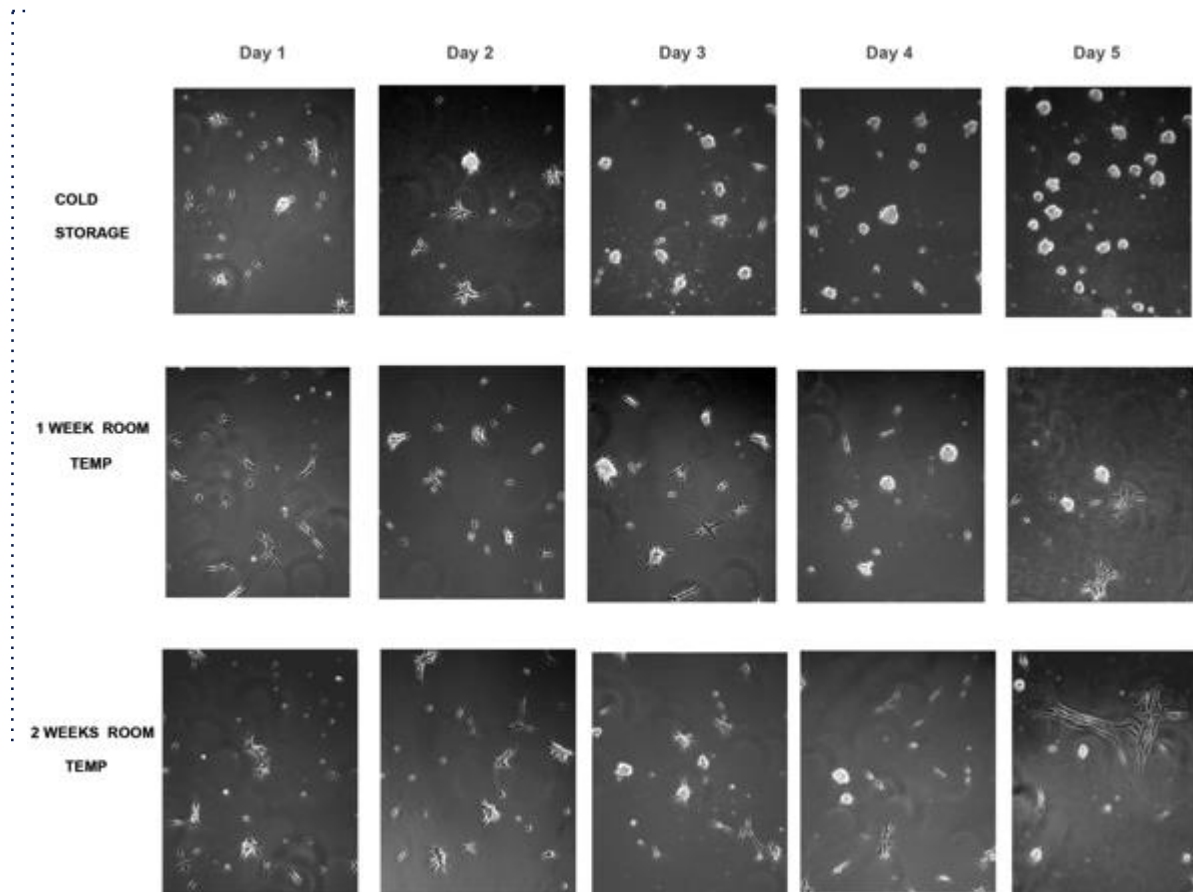
FITC-Labelled poly(K)



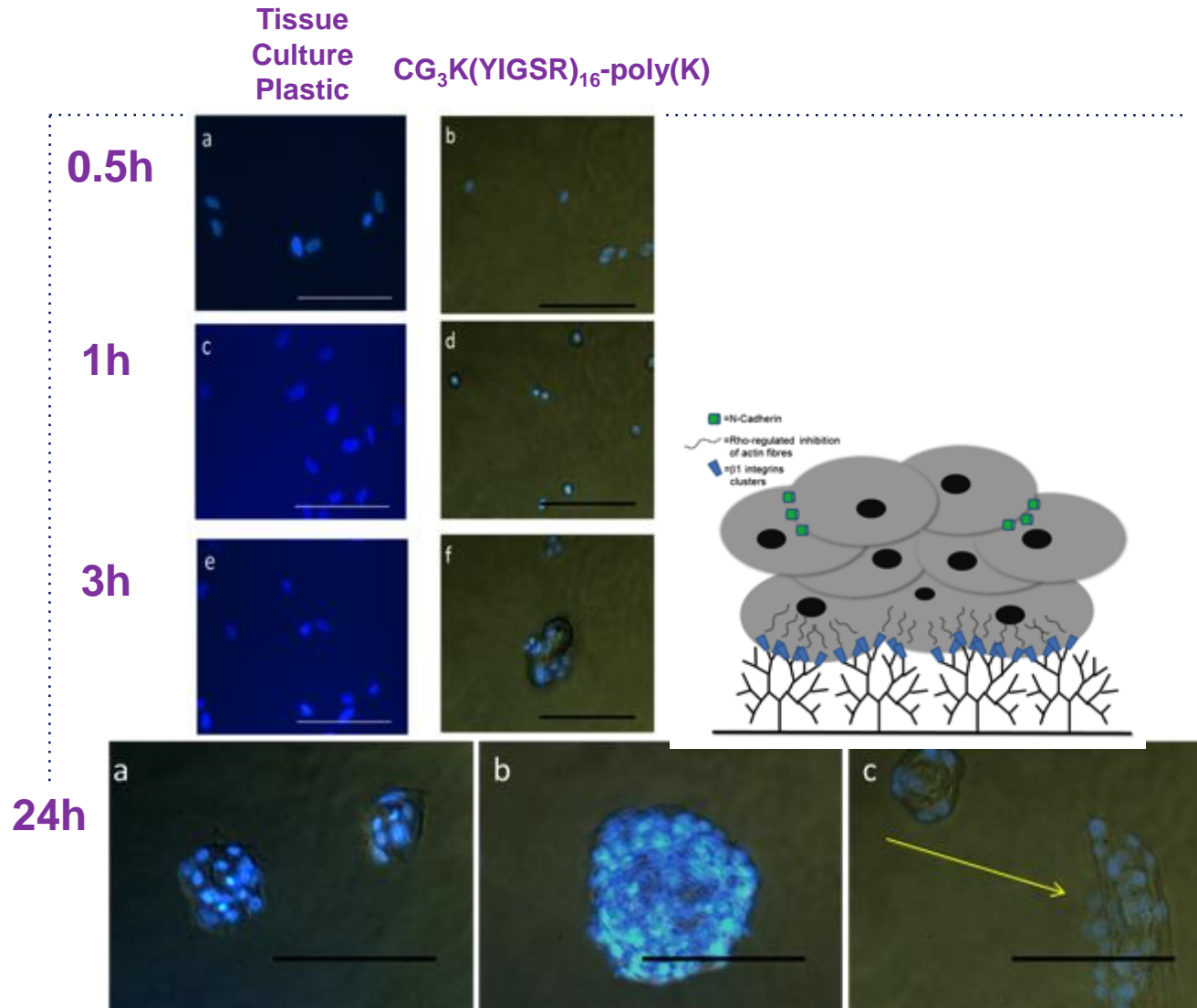
FITC-labelled
 $\text{CG}_3\text{K}(\text{YIGSR})_{16}$



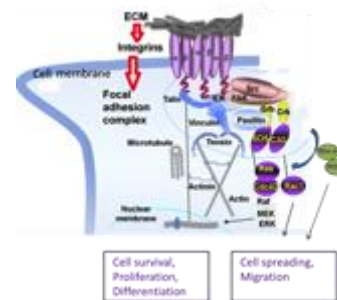
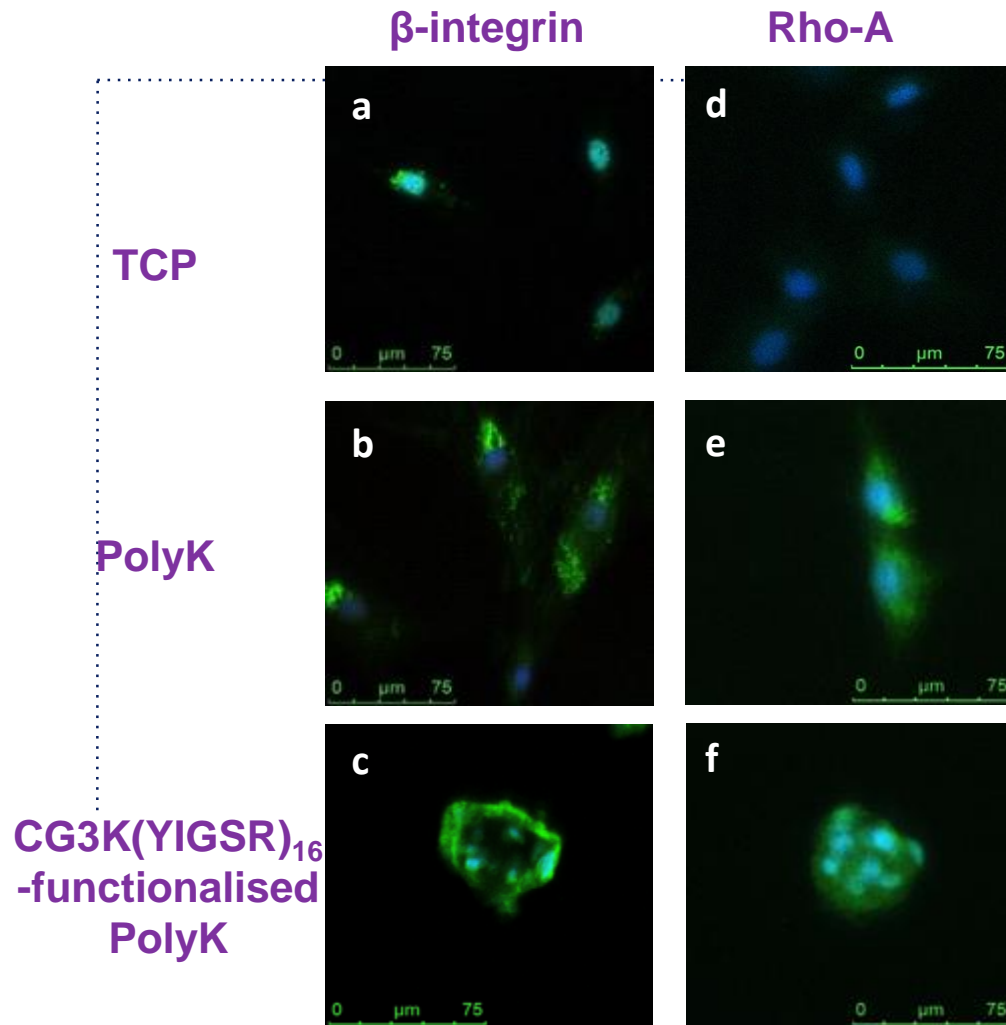
Mesenchymal Stem Cell Adhesion on $\text{CG}_3\text{K(YIGSR)}_{16}$ -tethered Poly(K) Substrate



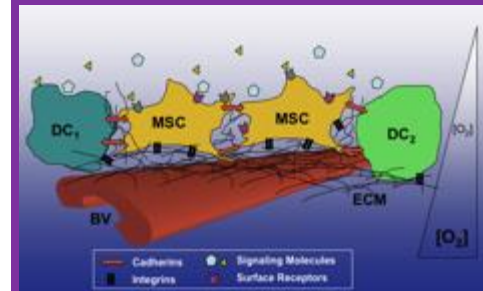
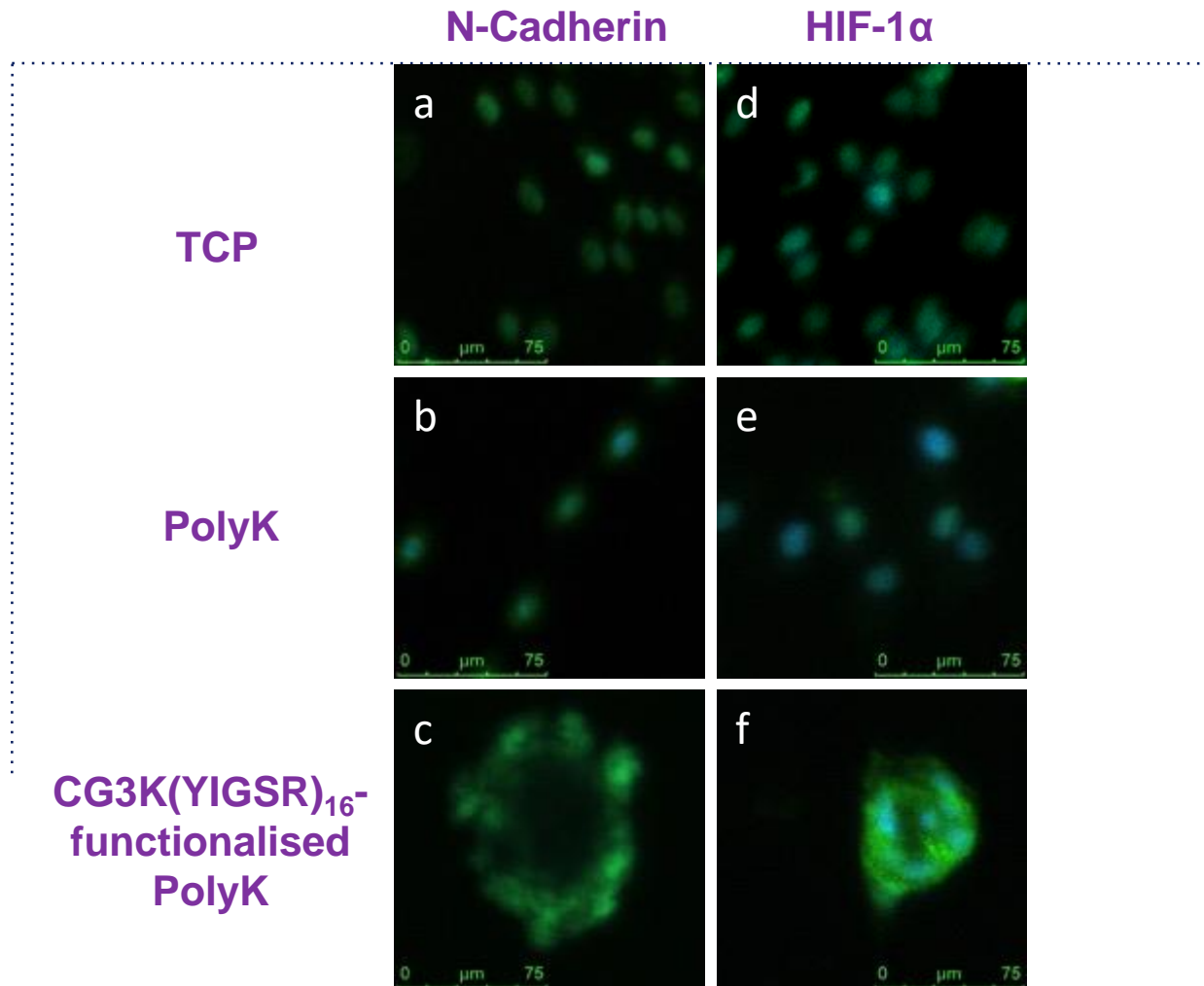
Mesenchymal Stem Cell Adhesion on $\text{CG}_3\text{K(YIGSR)}_{16}$ -tethered Poly(K) Substrate



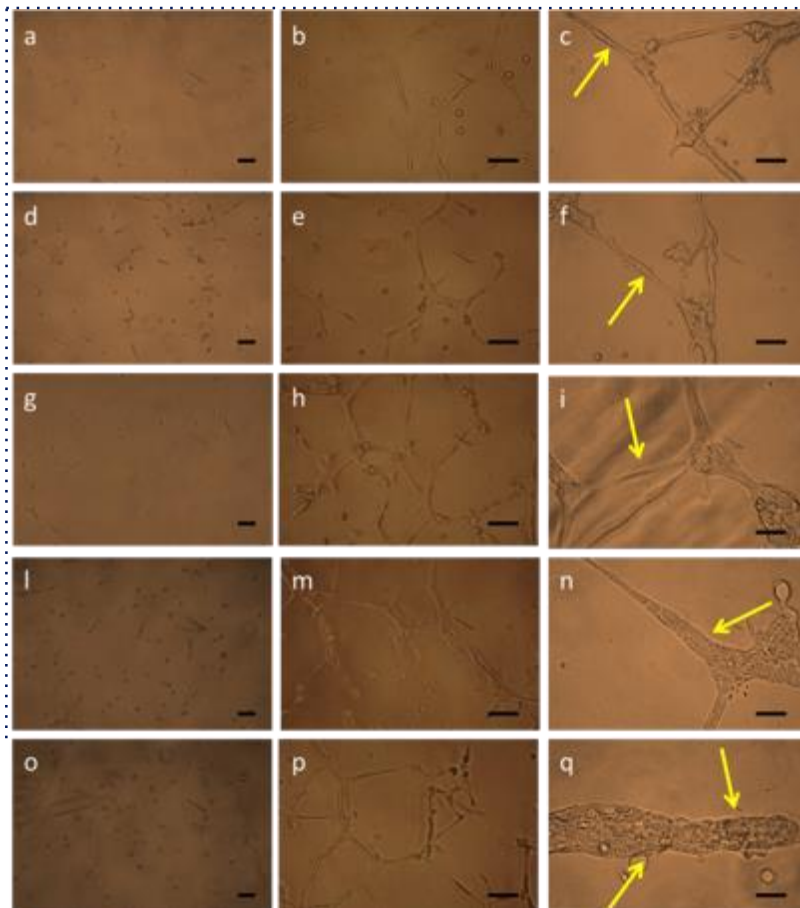
Integrin and Rho Expression and Localisation in Stem Cells Adhering on $\text{CG}_3\text{K}(\text{YIGSR})_{16}$ -tethered Poly(K) Substrate



Expression and Localisation of Migration and Hypoxia Markers in Stem Cells Adhering on CG₃K(YIGSR)₁₆-tethered Poly(K) Substrate



Stimulation of Endothelial Sprouting in 3D Matrigel by Supernatants of MSC Cultured on $\text{CG}_3\text{K}(\text{YIGSR})_{16}$ -tethered Poly(K) Substrate



2 days

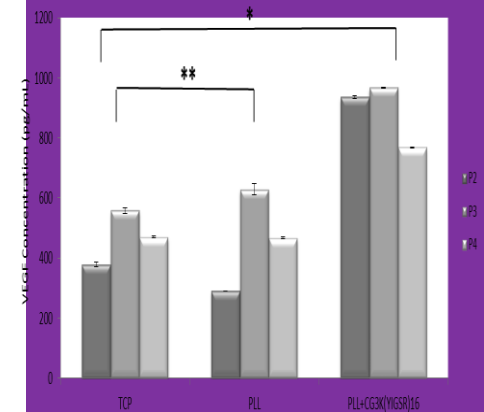
3 days

5 days

Tissue Culture
Plastic

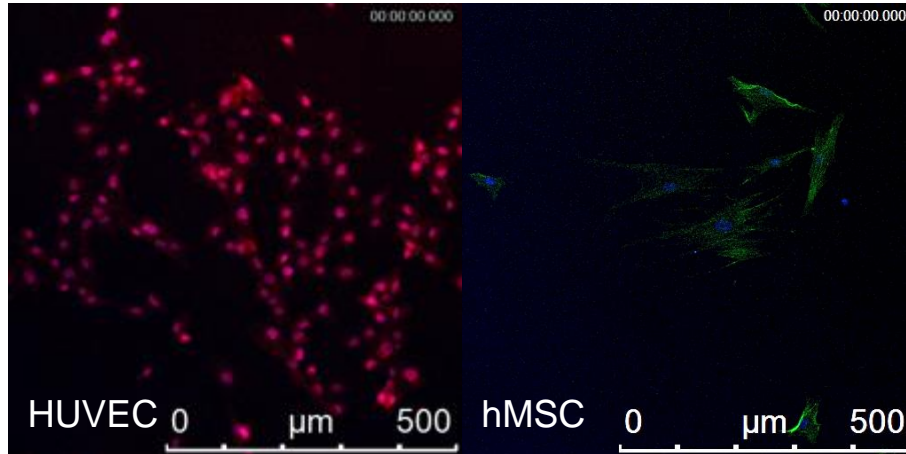
Poly(K)

$\text{CG}_3\text{K}(\text{YIGSR})_{16}$ -poly(K)



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Stimulation of Endothelial Sprouting on TCP by HUVEC/hMSC Co-Culture on $\text{CG}_3\text{K}(\text{YIGSR})_{16}$ -tethered Poly(K) Substrate

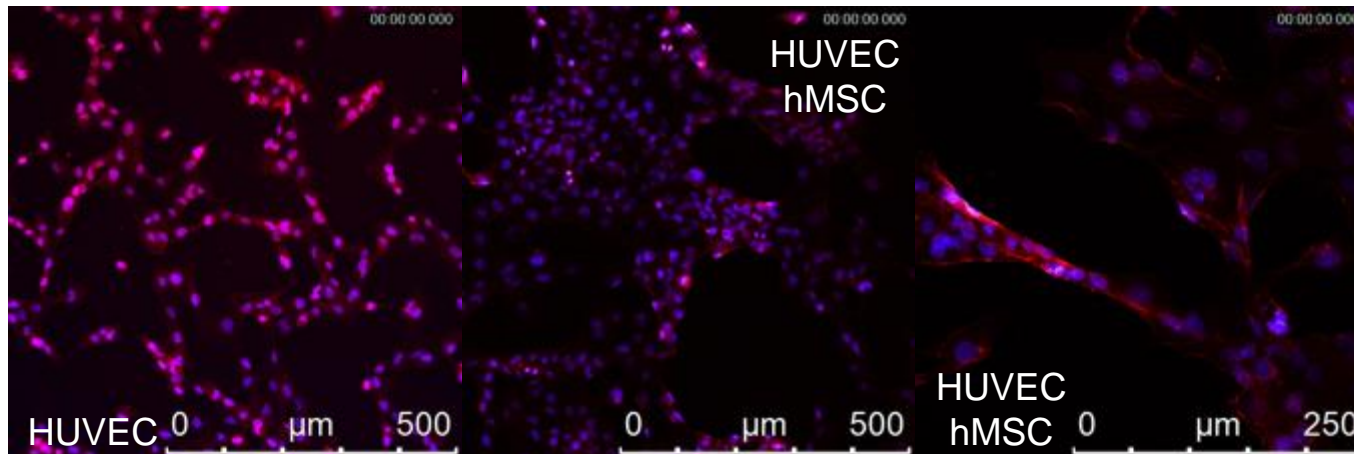


Tissue Culture Plate

CD31 = HUVEC

CD44 = hMSC

DAPI = Nuclei



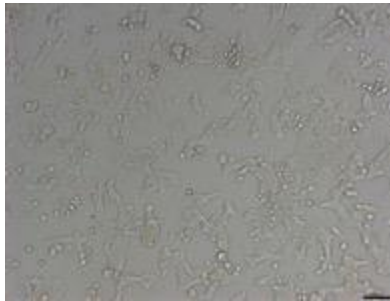
$\text{CG}_3\text{K}(\text{YIGSR})_{16}$ -tethered Poly(K) Substrate



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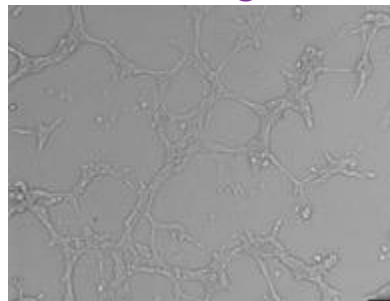
Beta Cells/Endothelial Cells Constructs

TC



Scale bar = 100µm

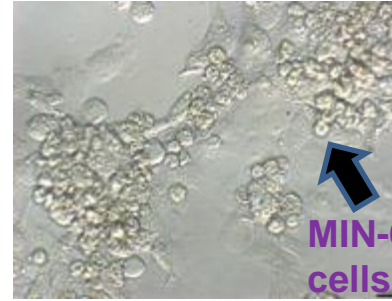
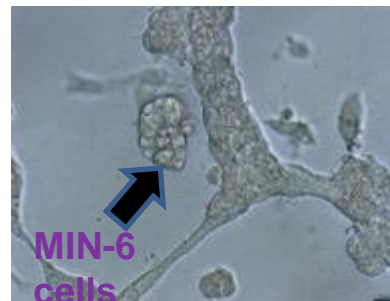
Matrigel



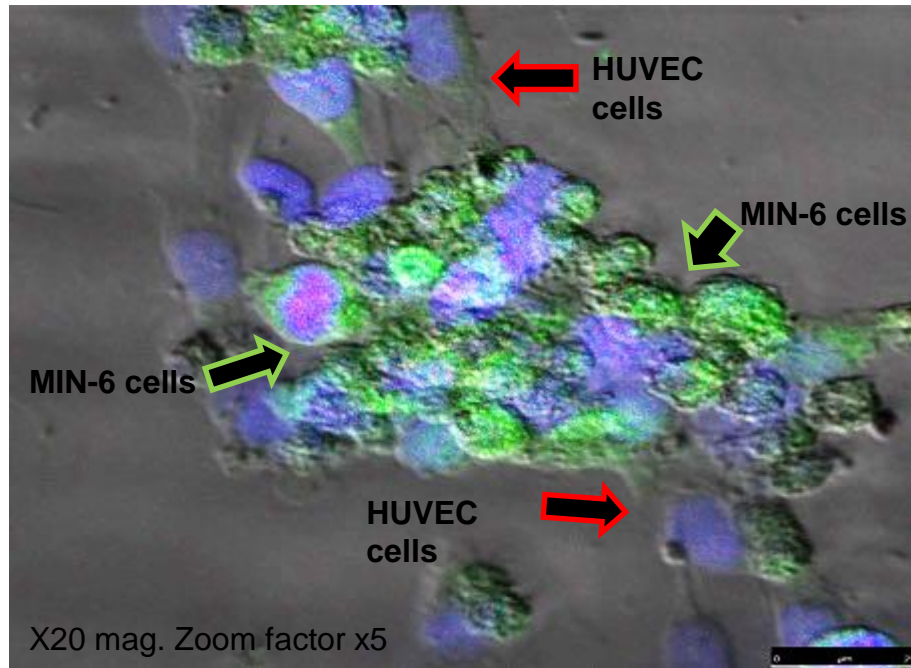
Dendron-modified
PLL



Scale bar = 50µm



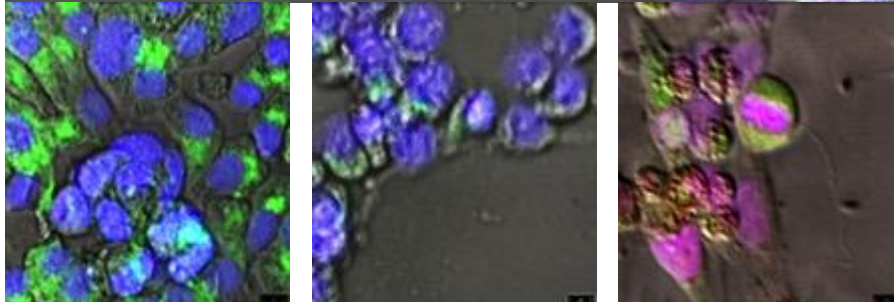
Beta Cells/Endothelial Cells Constructs



DAPI = nucleus
Insulin
CD31
(endothelial marker)

PLL-RG3K(YIGSR)16
20mins FBS free
TCP
FBS addition
40:60%
MIN-6: HUVEC
medium
24h

*Scale bar = 25µm

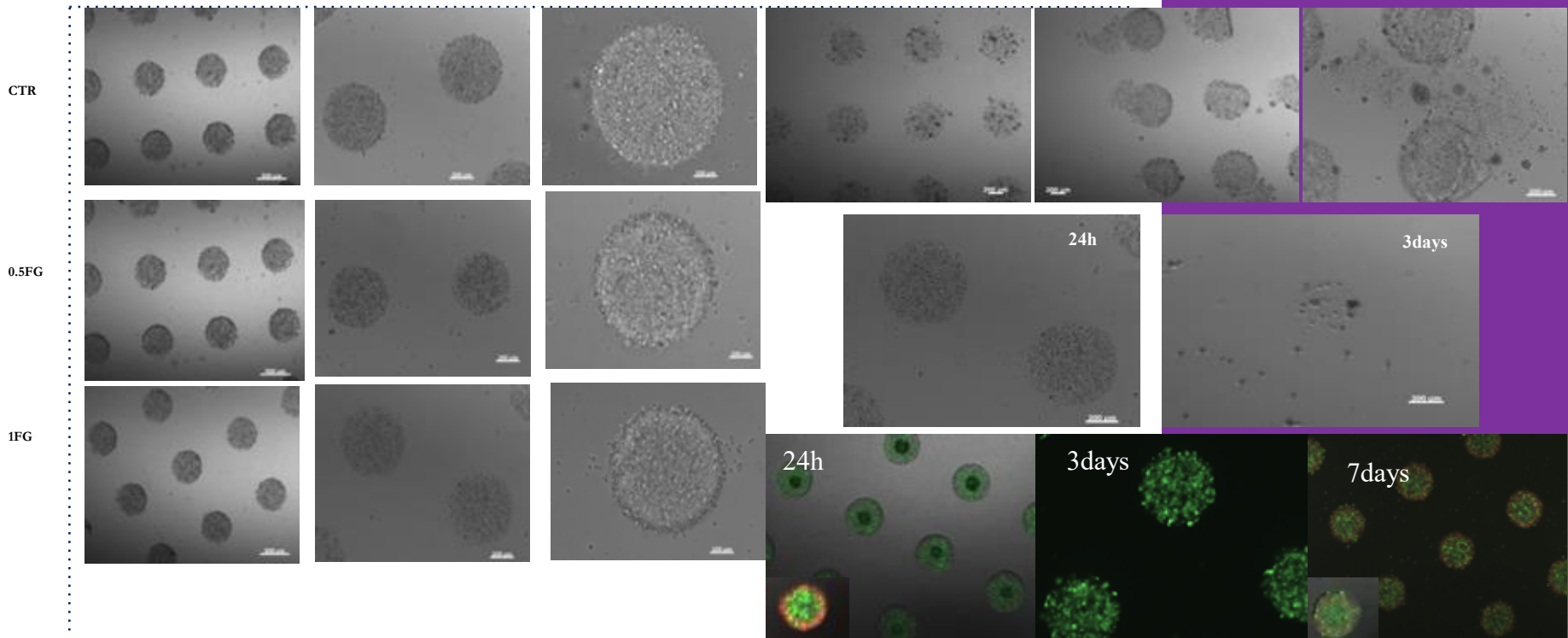


*Scale bar = 7.5µm



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Printed Neuro-mimicking Constructs



Neural Cells Printed in Gel-MA and Gel-Ma functionalised with different concentrations of CGen₃K(IKVAV)₁₆



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Phenodrive

| Phenodrive | Stem Cells | Endothelial Cells | Neural Cells | Epithelial cells | Osteoblasts | Chondrocytes | Haepatocytes | Cancer Cells |
|--------------------------|------------|-------------------|--------------|------------------|-------------|--------------|--------------|--------------|
| Integrin YIGSR | ✓ | ✓ | | ✓ | | | | |
| Integrin IKVAV | | | ✓ | | | | | |
| Integrin RGD | | | | ✓ | ✓ | | | |
| Universal Carboxybetaine | ✓ | | | | | ✓ | ✓ | ✓ |
| PS | | | | | ✓ | | | |
| Hypoxia | | | | | | ✓ | ✓ | ✓ |



www.tissueclick.com
info@tissueclick.com



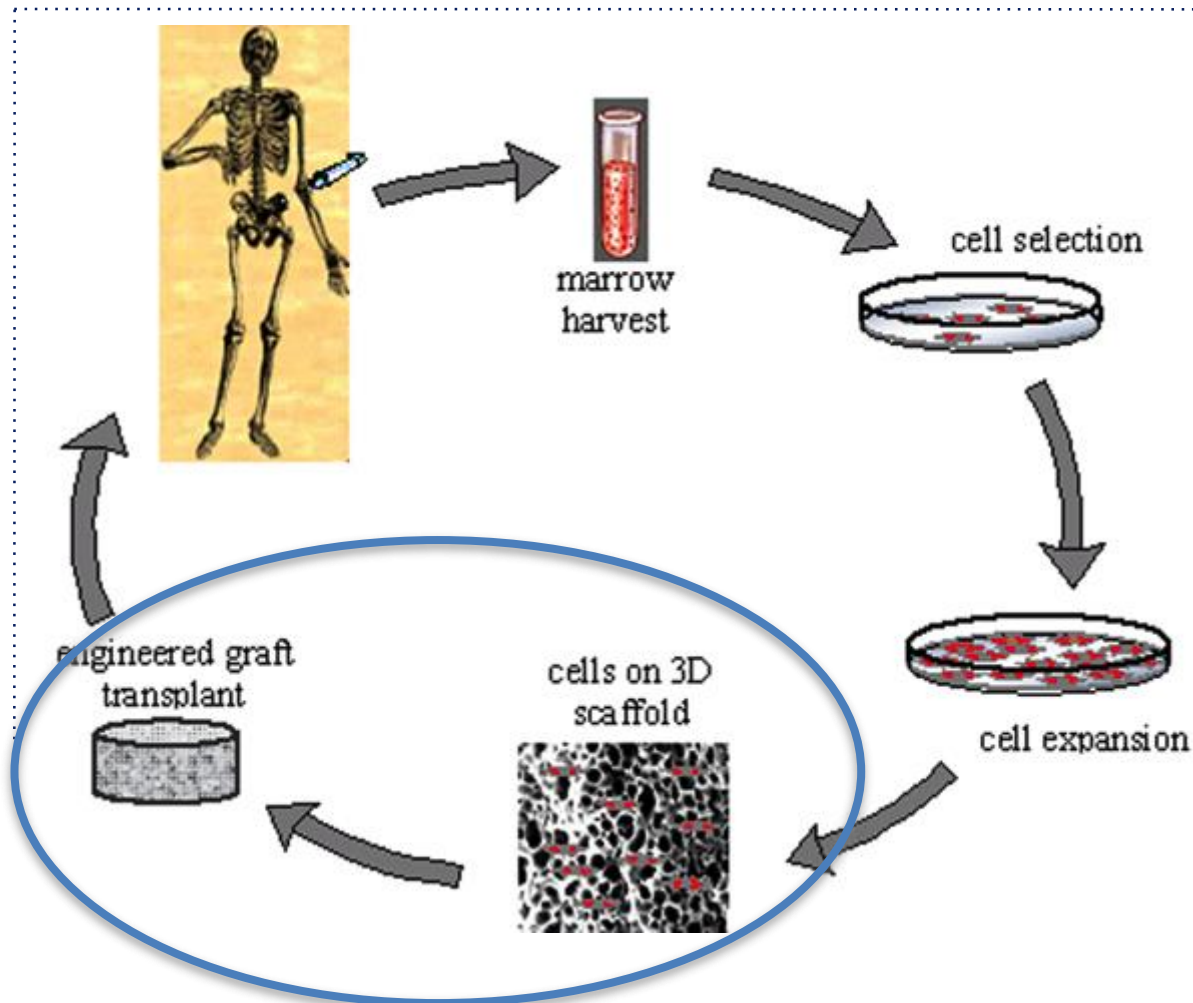
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Functionalisation of 3D Scaffolds for Osteochondral Defect Regeneration

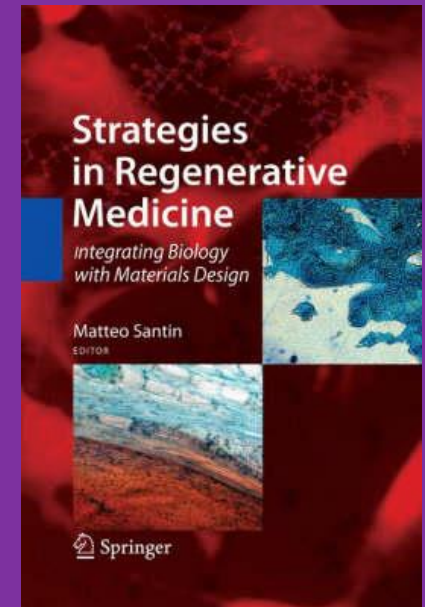


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The Tissue Engineering Paradigm

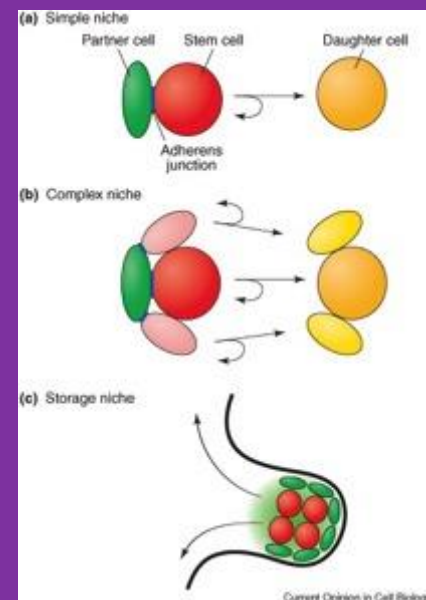
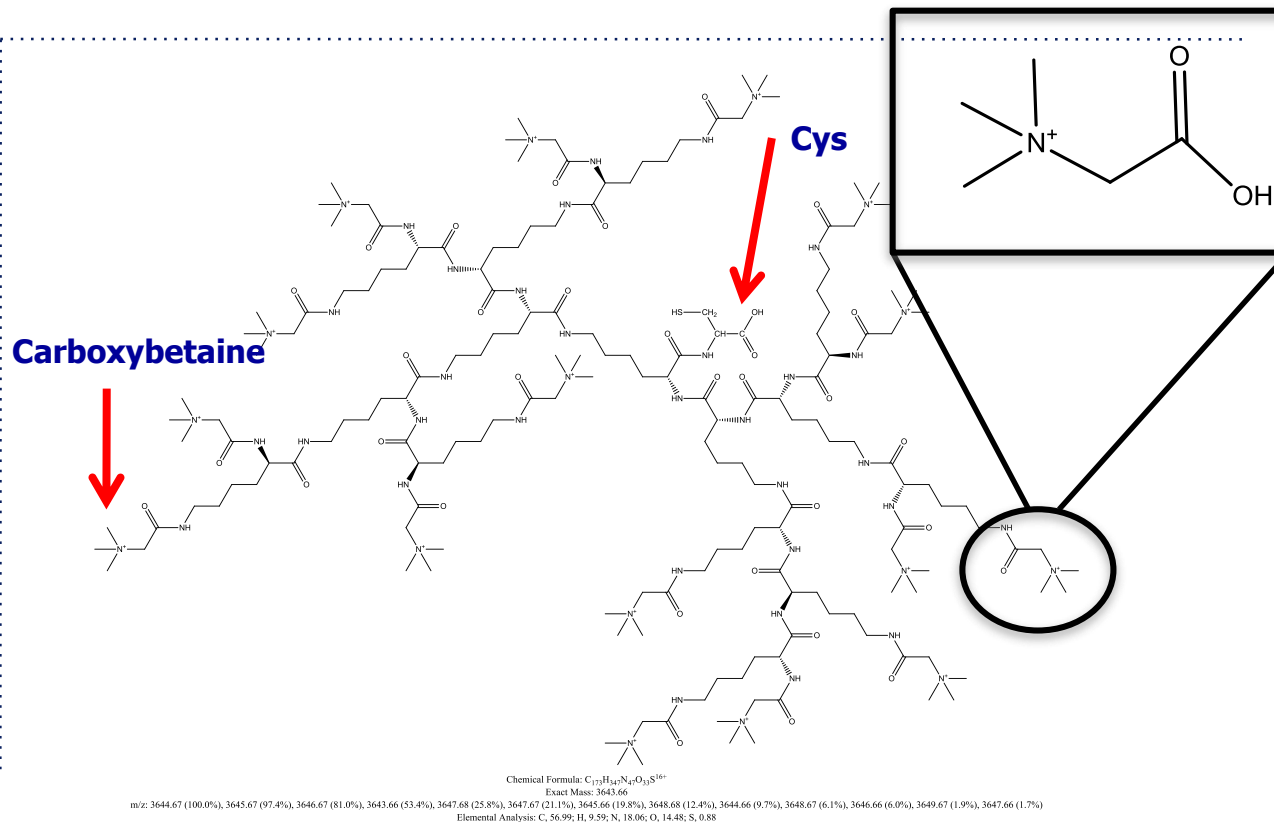


From Scaglione & Quarto
In *Strategies in Regenerative Medicine*
M Santin ed, Springer 2009, Chapter 15

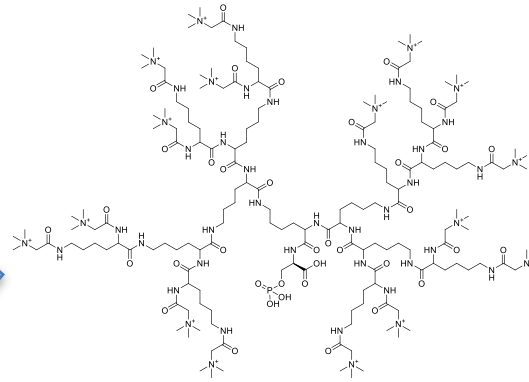


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Docking Site for Migrating/Loaded Stem and Differentiated Cells: The C G₃K(Carboxybetaine)₁₆ Unit



A diagram illustrating the flow of magma. At the bottom, a large yellow magma chamber is shown. A red arrow points upwards from this chamber into a vertical dike. A blue arrow points downwards from a vent at the top of the dike into the magma chamber, indicating a return flow of magma.



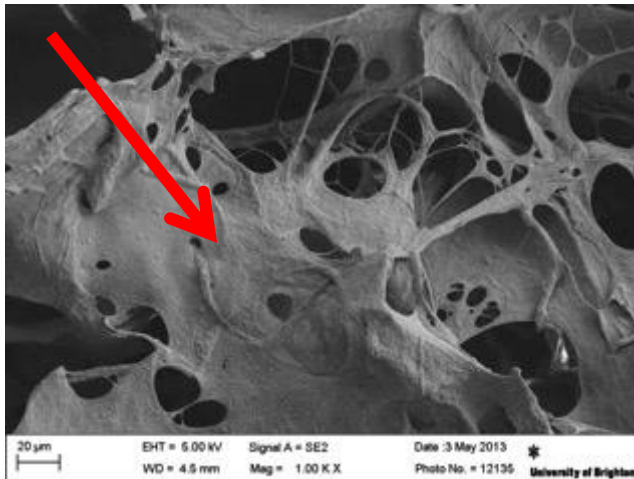
MaioRegen
Finceramica, Italy

An anatomical diagram of a knee joint in a sagittal view. The femur (thigh bone) is at the top, and the tibia (shin bone) is at the bottom. The patella (kneecap) is visible in the center. Three ligaments are highlighted with dashed lines and labeled with letters in circles: A points to the Anterior Cruciate Ligament (ACL), B points to the Posterior Cruciate Ligament (PCL), and C points to the Medial Collateral Ligament (MCL).

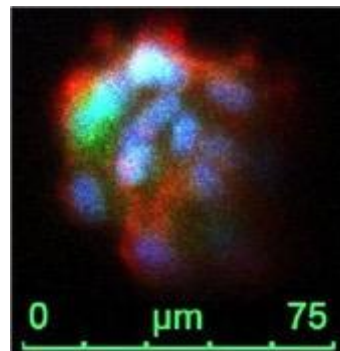
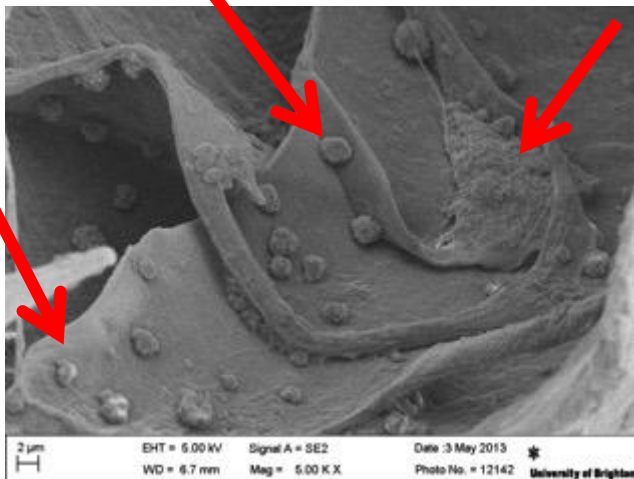


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Mesenchymal Stem Cell Organisation in Dendron-functionalised Scaffolds



MaioRegen
Finceramica, Italy



C G₃K (Carboxybetaine)₁₆⁻
MaioRegen



Surgery by
Dr E. Kon , Dr G.Filardo
IOR, Bologna,
Italy



University of Brighton

RAPID MAGNETISATION OF MESENCHYMAL STEM CELLS

Nunzia Di Maggio^{1*}, Elisa Martella^{2,3*}, Steve Meikle⁴, Marta Columbaro⁵, Enrico Lucarelli², Matteo Santin^{4†} and Andrea Banfi^{1†}

Rapid and efficient magnetization of mesenchymal stem cells by dendrimer-functionalized magnetic nanoparticles, Nanomedicine 2016, DOI 10.2217/nnm-2016-0085

¹Cell and Gene Therapy, Department of Biomedicine, Basel University and Department of Surgery, Basel University Hospital, Basel, Switzerland, ²Osteoarticular Regeneration Laboratory, Rizzoli Orthopaedic Institute, Bologna, Italy

³Department of Biomedical and Neuromotor Sciences (DIBINEM), University of Bologna, Italy

⁴BrightSTAR, Brighton Centre for Regenerative Medicine, University of Brighton, UK

⁵Musculoskeletal Cell Biology Laboratory, Rizzoli Orthopaedic Institute, Bologna, Italy



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Stem Cell Magnetisation

- Intraoperative production of tissue-engineered graft
 - isolation of multipotent progenitors from a patient,
 - their seeding on an appropriate scaffolding material
 - their re-implantation in a single-step procedure directly in the operating room

Mehrkens A, Saxer F, Guven S, *et al. Eur. Cell. Mater.* 24, 308–319 (2012).

- Magnetic scaffolds have been recently developed and cell magnetization can be exploited to rapidly and consistently drive cells into the scaffold prior to transplantation.

Yun H-M, Ahn S-J, Park K-R, *et al. Biomaterials.* 85, 88–98 (2016).



Cell Magnetisation by Superparamagnetic nanoparticles

- Coupling of cells to superparamagnetic nano-particles (MNP) can confer a magnetic drive to the cells
- Cell labelling with MNP is a slow and low-yield process (12 to 24 h) often not able to guarantee levels of magnetization sufficient for cell manipulation
- MNP (from 5 to 150 nm in diameter) can be coated with different polymeric materials (e.g. dextran, polylysine, chitosan or silica) to enhance their biocompatibility and promote their endocytosis

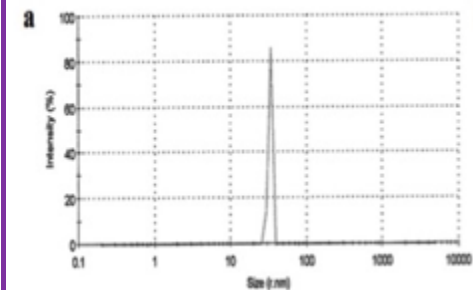
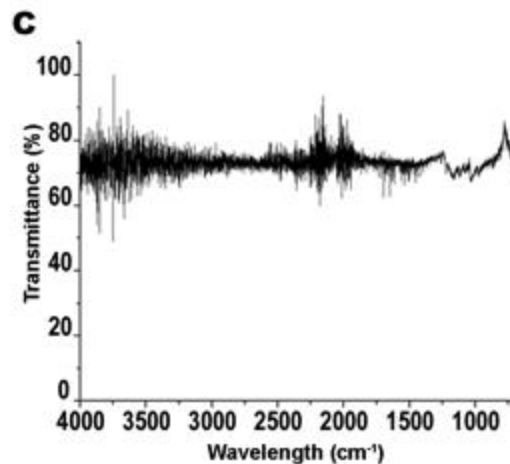
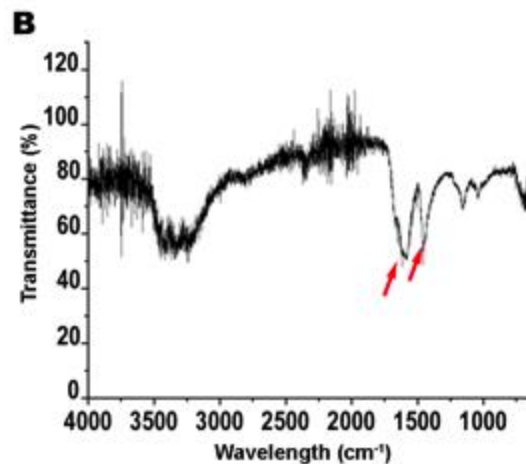
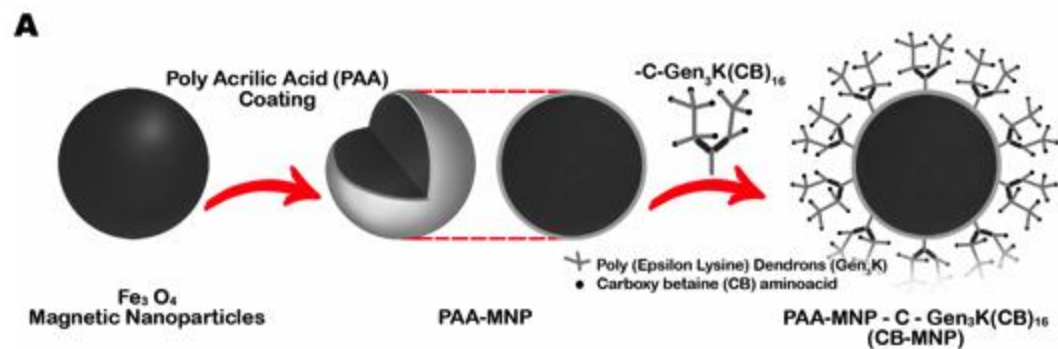


Materials and Methods: Optimised CG3KCB₁₆MNP@PAA manufacturing

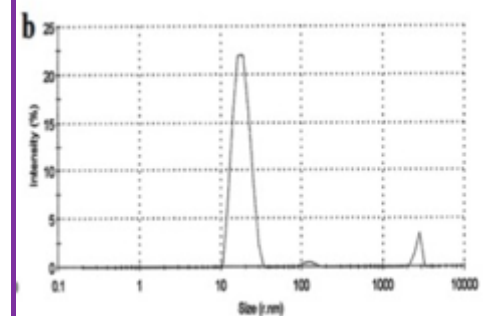
- PAA@MNP were functionalised with Cys via formation of an amide bond using carbodiimide/N-hydroxysuccinimide chemistry (4:1) ratio in 0.1 MES buffer for 1 hour in a shaking incubator (100 rpm, room temperature)
- Cys was added for 1 hour in a shaking incubator (100 rpm, room temperature). Supernatant was removed and beads washed with ethanol and air dried.
- CG3KCB₁₆ dendron was attached to PAA@MNP -Cys-SH via formation of –S-S- by 3 % H₂O₂ treatment for 2 hours. Supernatant removed and samples air dried
- Physico-chemical characterisation was performed



PAA@MNP Functionalisation by carboxybetaine-tethered poly(ϵ -lysine) dendrons



Size= 33.37 nm
Zeta Pot = -25.6 mV

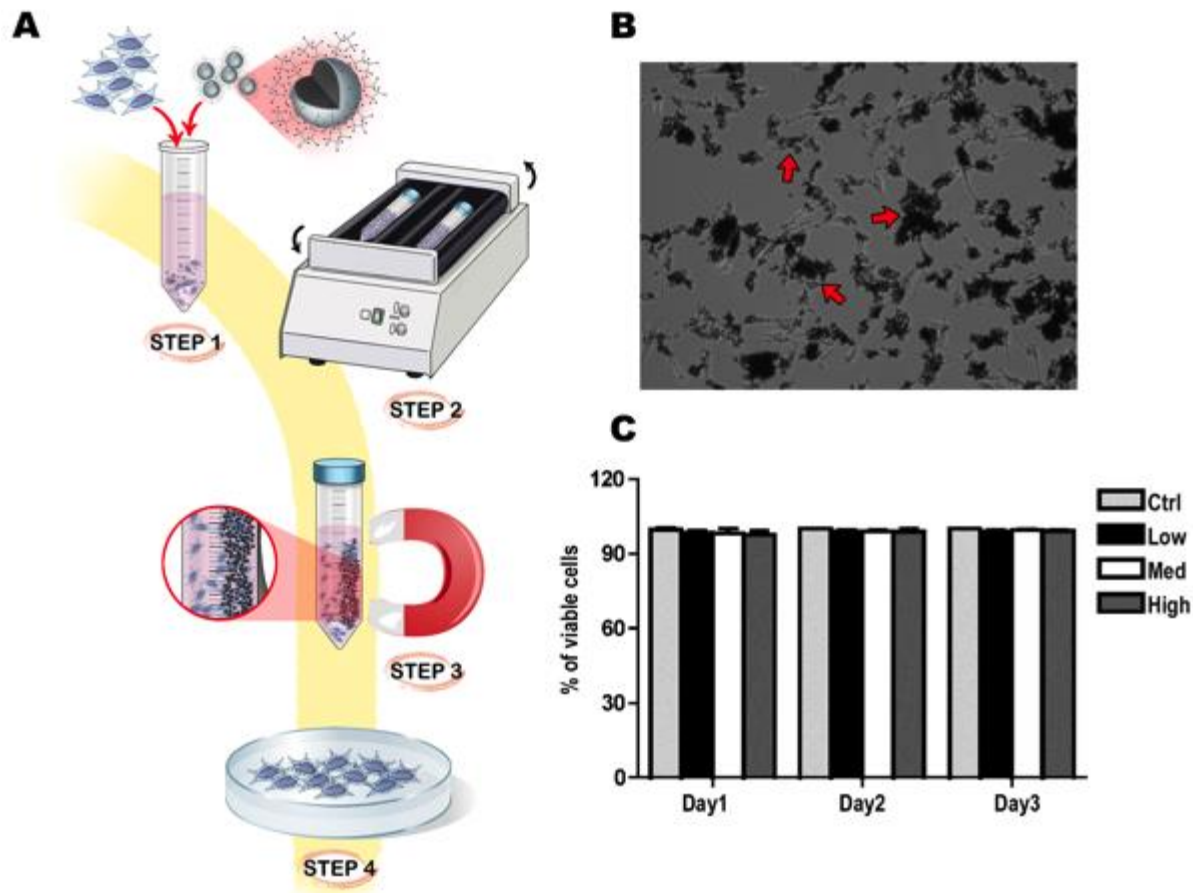


Size= 18.46 nm
Zeta Pot = -45.6 mV



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Mesenchymal Stem Cell Labelling with MNP

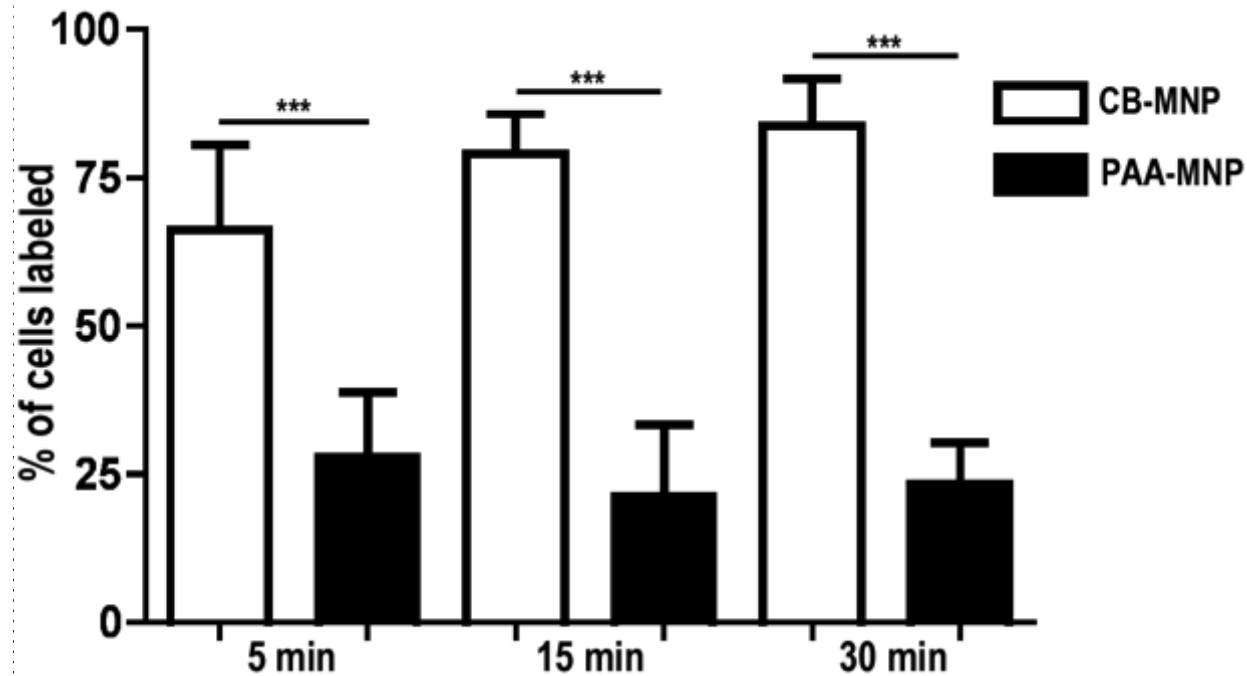


low = $7.2 \mu\text{g}/10^4$ cells
medium = $14.4 \mu\text{g}/10^4$ cells
high = $28.8 \mu\text{g}/10^4$ cells

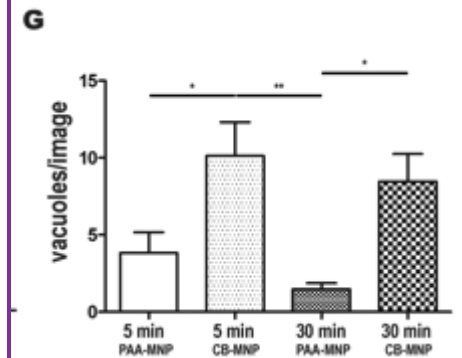
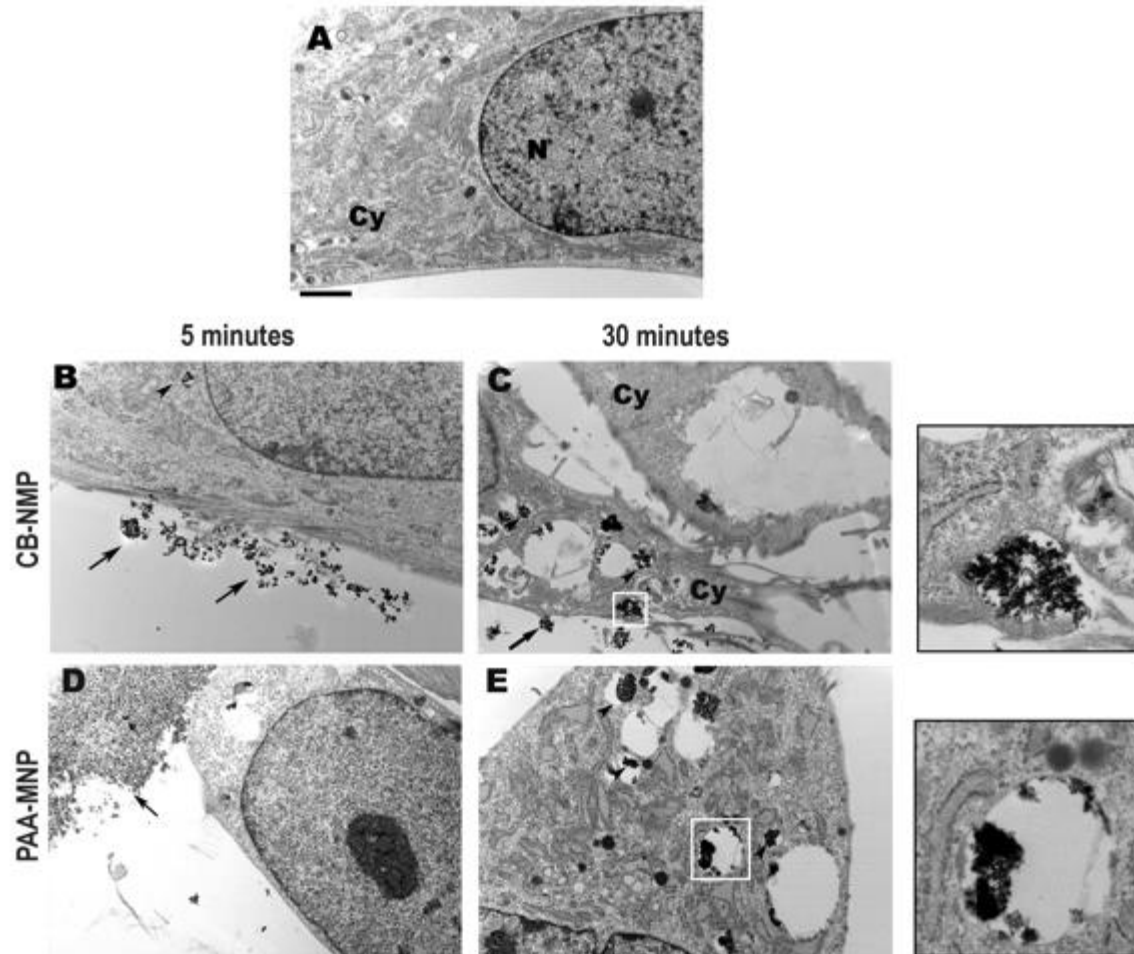


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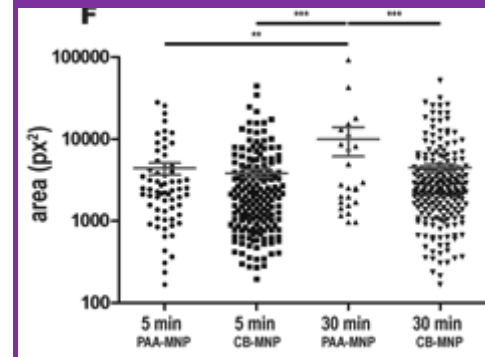
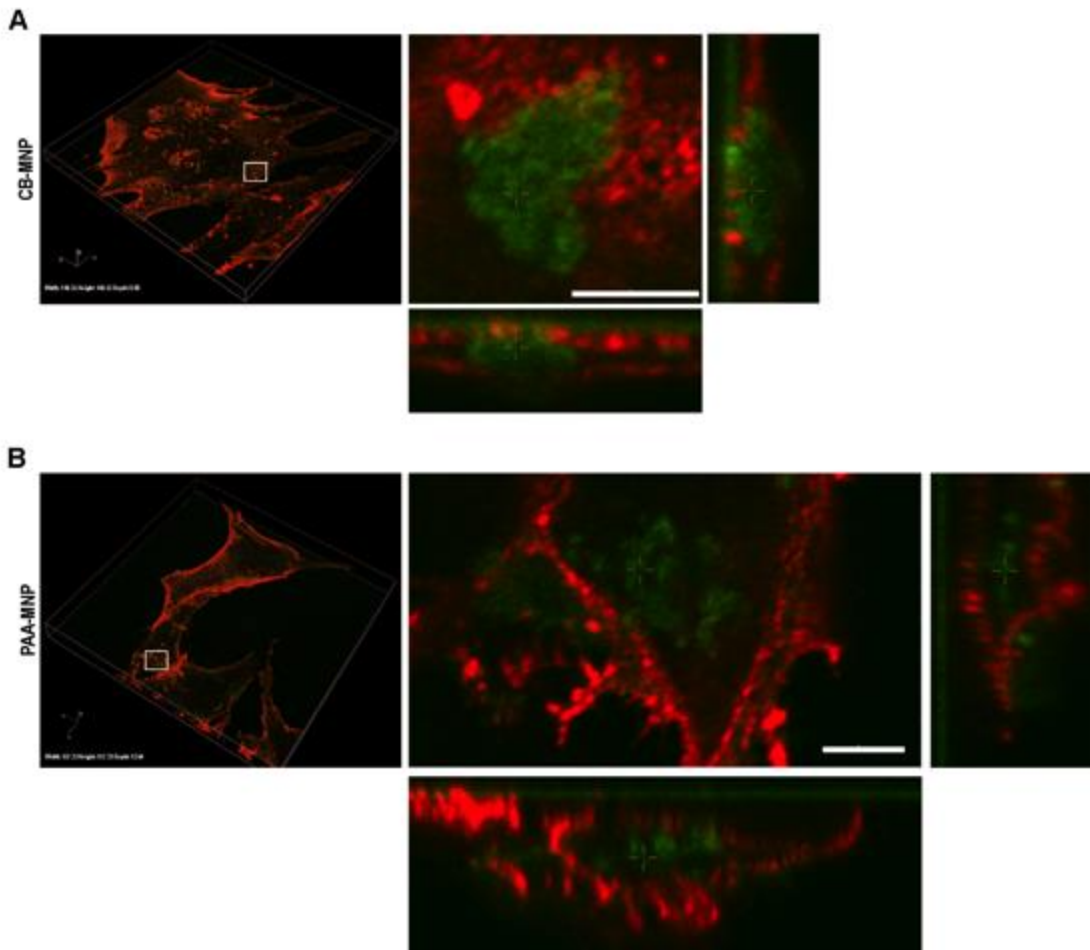
Mesenchymal Stem Cell Labelling with MNP



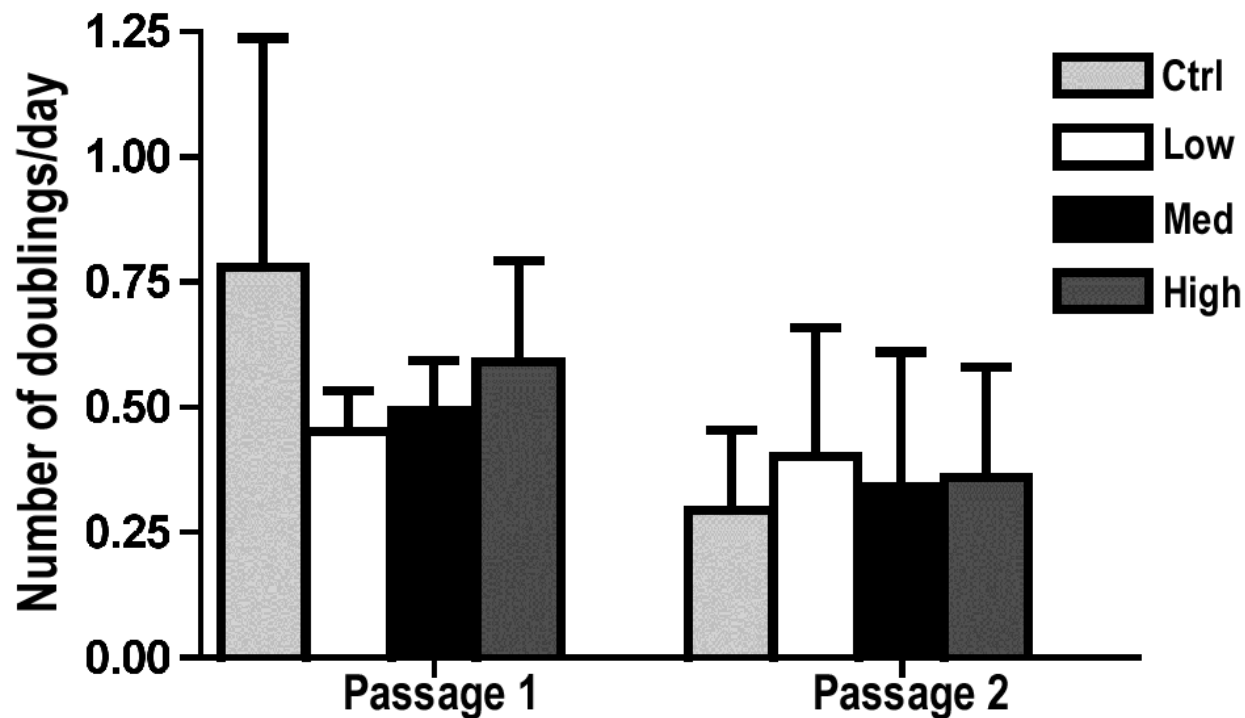
Mesenchymal Stem Cell Labelling with MNP: TEM Analysis



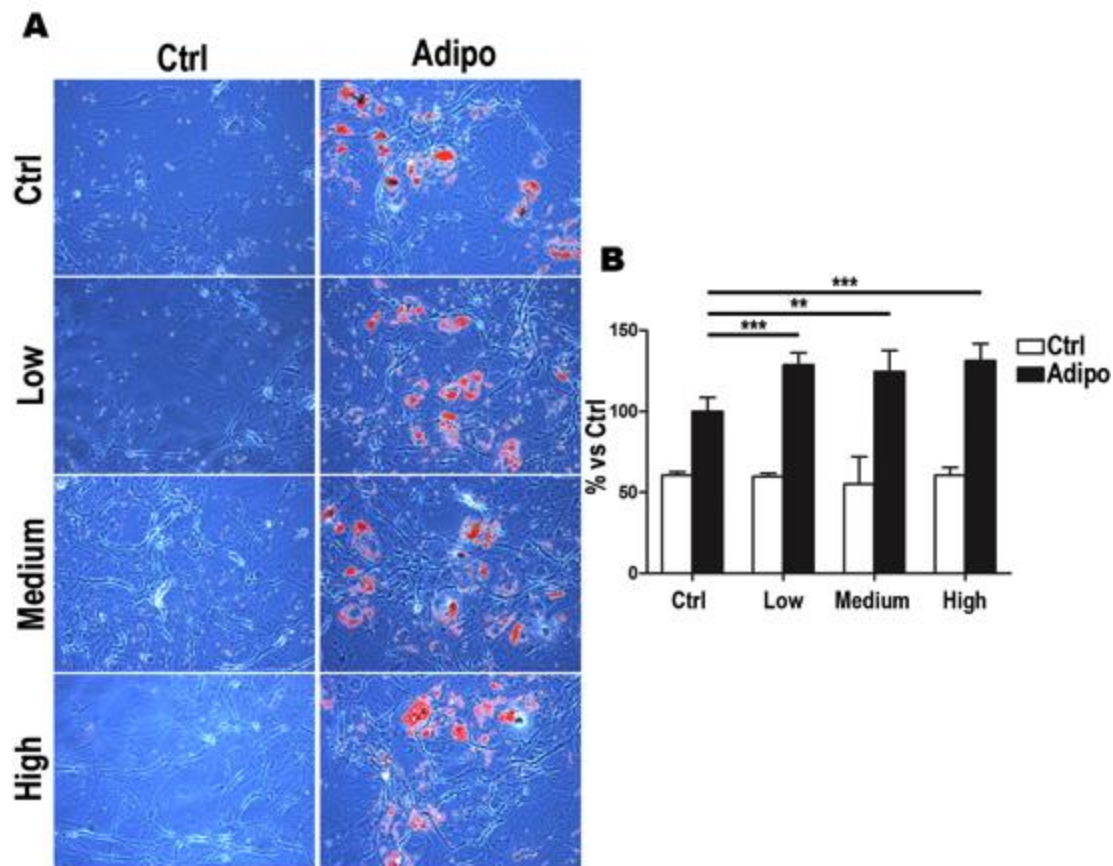
Mesenchymal Stem Cell Labelling with MNP: Confocal Analysis



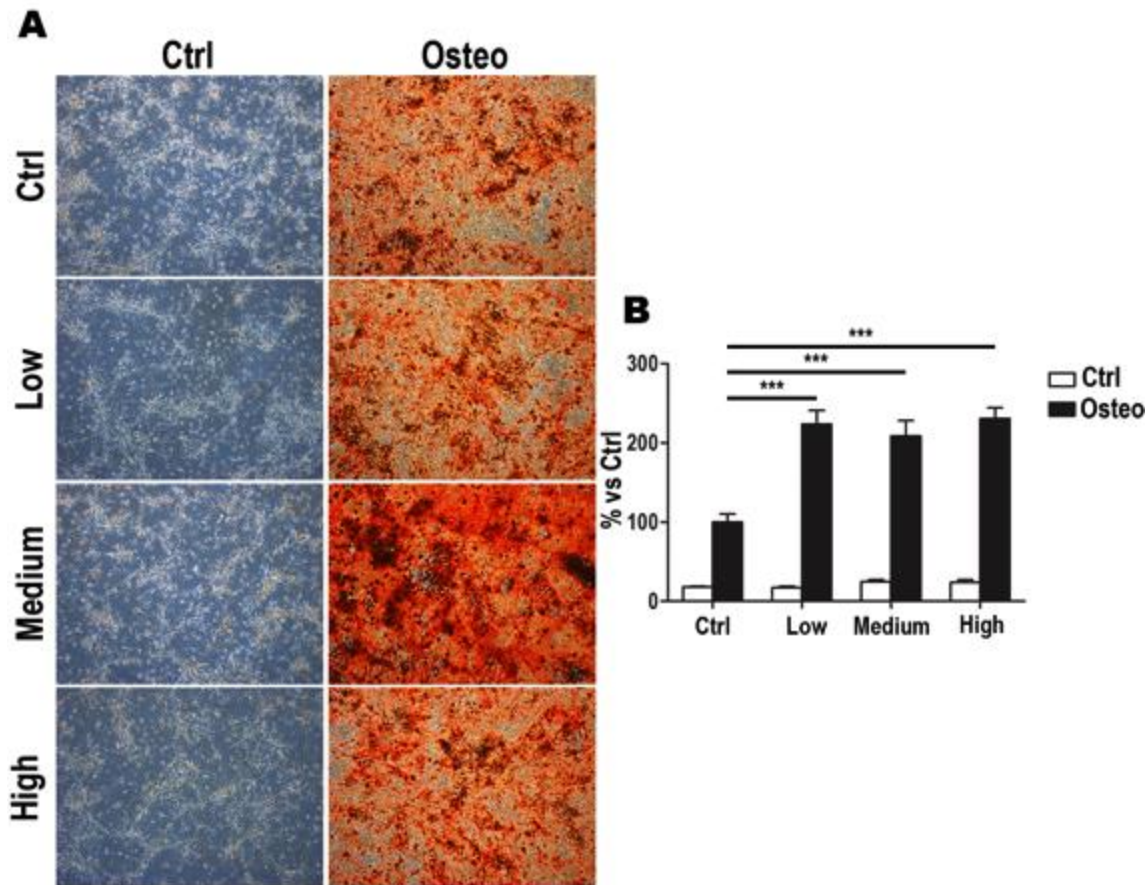
Mesenchymal Stem Cell Labelling with MNP: Population Doubling



Mesenchymal Stem Cell Labelling with MNP: Adipogenic Differentiation



Mesenchymal Stem Cell Labelling with MNP: Osteogenic Differentiation



Conclusions

- Synthetic Extracellular Matrix Analogues can be achieved by macromolecular design, scaled-up batches and **GMP conditions**
- EMA can be exploited as
 - Specialised substrates for cell pre-clinical handling of cells
 - more complex **clinically-reflective in vitro models** including different types of cells and integrated testing the safety/efficacy of drugs and other products in a regenerative niche
 - Functionalisation of 3D scaffolds
 - Bioink for additive manufacturing adding biofunctionality to a variety of more established polymers



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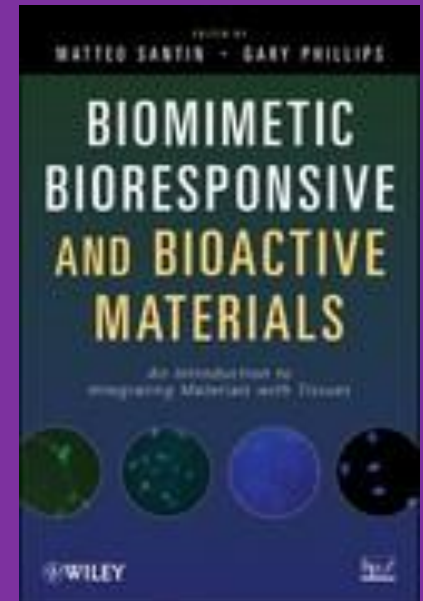
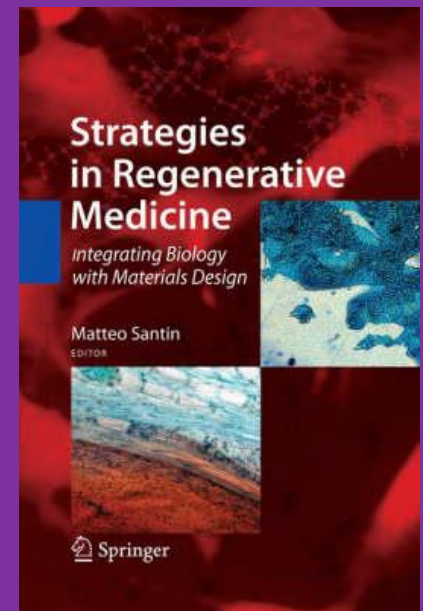
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Save the Date

Important dates

| | |
|------------------------------------|-----------------|
| On-line registration opens: | 1 December 2016 |
| On-line abstract submission opens: | 1 December 2016 |
| Abstract Submission deadline: | 31 January 2017 |
| Notification to authors: | 20 May 2017 |
| Early-bird registration deadline: | 31 May 2017 |

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